Research Article

Toneburst Vestibular Evoked Myogenic Potential (VEMP) in Patients with Ménière's Disease

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Abstract

Objective: In this study, we test the hypothesis that the cochlear hydrops of Meniere's syndrome leads to alteration in saccular motion that change the dynamics of the vestibular evoked myogenic potential. Study Design: Prospective cohort study. Setting: A university hospital. Subjects: Twenty normal adult volunteers and $\gamma \circ$ adult patients with unilateral Meniere's disease by American Academy of Otolaryngology-Head and Neck surgery diagnostic criteria. Intervention: All subjects underwent vestibular evoked myogenic potential testing using ipsilateral broadband click and short tone burst stimuli at over and vere Hz. Main Outcome Measure: P'-N' corrected amplitude, P' and N' latency. V···/o·· FPA ratio, AR, IAL difference, Results: Normal subjects show a frequency dependent vestibular evoked myogenic potential with best response (frequency tuning) at over Hz. Compared with normal subjects and unaffected ears of Meniere's subjects. Affected Meniere's ears showed frequency shift and there was less tuning apparent at ovv Hz. Unaffected ears of Meniere's subjects also showed affected frequency tuning. Both Meniere's ear and other ear FPA ratio was larger compared to control ears while no statistically significant difference between Meniere's ear and other ears. Conclusion: Meniere's ears display alteration in vestibular evoked myogenic potential tuning, supporting our hypothesis of altered saccular motion mechanics arising from hydropic distention. Unaffected ears of unilateral Meniere's subjects show similar changes but to lesser degree. This finding may be because of occult saccular hydrops in the asymptomatic ear or binaural interaction in the vestibular evoked myogenic potential otolith cervical reflex arc.

Key Words: Toneburst, Vestibular, Evoked, Myogenic Potential

Introduction

The Vestibular evoked myogenic potential (VEMP) is a large, short latency, myogenic potential produced by contraction of the sternocleidomastoid (SCM) muscle in response to loud acoustic stimulus^[1]. Studies have shown that 9.-1.. dB nHL click or toneburst stimuli produce optimal VEMP recording. However, Low frequency tone burst stimuli give more pronounced results than click or other frequencies^[¹]. The VEMP has been applied clinically to evaluate the integrity of the sacculocollic reflex and is widely clinically applicable in many disease as Ménière's disease (MD), superior semicircular canal dehiscence, large vestibular aqueduct syndrome, acoustic neuroma, multiple sclerosis and brainstem stroke^[^r].

It has been reported that VEMP may be useful in assessing MD because the saccule, next to the cochlea is the second most frequent site of hydrops formation^[1].</sup> According to stage of MD. VEMP may take different forms either enhanced, decreased amplitude or absent. Furthermore, Rauch et al..^[°] reported the alteration of tuning characteristics of VEMP in MD patients. They reported that, in healthy subject, the largest amplitude and the lowest threshold were obtained to ••• Hz toneburst. whereas patients with MD showed less tuning at ovv Hz and shift of the best frequency to '... Hz. This result was based on their findings that the ratio of the amplitude of P'-N' of VEMP of ov Hz stimulus to that of V··· Hz was significantly less in Ménière's patients than

in normal subjects. Rauch et al attributed this shift to change of resonant frequency in the saccule and suggest that amplitude relation of VEMP at or Hz to Your Hz may help in staging, diagnosis of early Ménière's, diagnosis in other ear and confirm diagnosis of probable Ménière's.

The current work was designed to study VEMP in patients with MD using click and tonebursts with ••• and •••• Hz. The specific aims of the current work were:

 1 - To determine VEMP findings in MD patients and compare the findings with those of healthy control subjects. The specific parameter of interest is the frequency peak amplitude (FPA) ratio, which is ratio of P¹-N¹ VEMP amplitude at 1 ··· Hz toneburst to P¹-N¹ VEMP amplitude at $^{\circ}$ ·· Hz toneburst.

Y- To determine if VEMP can diagnose the involvement of the other ear in MD patients.

Subjects

The current study included \checkmark groups. Group I was the group of Meniere's patients, which included $\checkmark \circ$ patients with definite MD. group II was the control group, which included $\curlyvee \cdot$ healthy volunteers.

I- Patients with definite MD were selected according to the criteria of AAO/HNS [^Y] which are

A- Two or more definitive spontaneous episodes of vertigo Υ· minutes or more. B- Audiometrically documented hearing loss on at least one occasion.

C- Tinnitus or aural fullness in the treated ear.

D- Other causes excluded.

II- Subjects in the Control group were selected according to the following criteria

A- No history suggestive for vestibular disorder as vertigo, dizziness, or sense of imbalance.

B-No history suggestive for migraine as migrainous headache, phonophobia and photophobia.

C-Bilateral normal hearing sensitivity.

D- Bilateral normal tympanograms with intact acoustic reflex and no current or history of middle ear disease.

E- Normal cochlear function, as shown from normal DPOAE.

F- No history of medical disorders known to affect hearing as diabetes, hypertension.

Methods

All subjects were subjected to:

I- Full history taking:

History included description of the vertiginous attack, frequency of attack, duration of each attack, condition of the patients in between attacks, degree of disability during attack, associated hearing loss and tinnitus, sense of ear fullness, nausea and vomiting.

II- Otoscopic examination.

III- Audiological evaluation in the form of:

1- *Immittancemetry* using Zodiac \pounds immittancemeter (GN Otometrics A/S, Taastrup, Denmark) to measure middle ear pressure and stapedial muscle reflex threshold at frequencies of $\circ \cdots$, $1 \cdots , 7 \cdots$ and $\pounds \cdots$ Hz and to exclude middle ear pathologies.

Y- Pure tone audiometry using Amplaid γ . audiometer (Amplus Corp. Boulder, CO, U.S.A.) and sound treated room (amplisilence) to assess hearing sensitivity. Air conduction threshold was obtained for the frequency range $\gamma \circ \cdot - \wedge \cdot \cdot \cdot$ Hz at single octave intervals using a TDH ξ^{9} ear phone (Telephonics Corporation, Farm ingdale, NY, U.S.A.), while bone conduction threshold was obtained for the frequency range $\circ \cdot \cdot - \epsilon \cdot \cdot \cdot$ Hz at single octave intervals using a BV1 bone vibrator (Radioear, New Eagle, PA, U.S.A.). Speech reception threshold (SRT) and speech discrimination score using bisyllabic and monosyllabic phonetically balanced words respectively.

 $\tilde{\gamma}$ - **DPOAE** using the Intelligent Hearing system (IHS) two channel evoked potential recording apparatus with Smart OAE £.º software (Intelligent Hearing Systems, Miami, FL, U.S.A.). Two tones were used: $L^{1}=0$ dB SPL and $L^{1}=0$ dB SPL, while f^{γ}/f^{γ} was $\gamma.\gamma\gamma$. Both the amplitude of response of the distortion product (DP) at $f^{-}f^{-}$ and background noise (Ns) were obtained at nine points corresponding to f⁷ frequencies of 00^m, VAT, 11.0, 107., TT11, TITO, ££17, 770. and AATY Hz. These measurements were used to build a DPgram by displaying the DP against the f^{γ} frequency. The signal to noise ratio (SNR) was measured (SNR=DP-Ns) at each of these nine points. DPOAE was considered normal (pass), thereby reflecting normal cochlear function, if the SNR was >^TdB SPL on at least $\vee \cdot$ [?]. of the tested frequencies^[1].

E- ABR using IHS with smart evoked potentials software version *£.°*. The stimuli were \cdots us alternating click delivered through head phone at intensity level of \wedge .-9. dB nHL with repetition rate of the stimuli was *Y*) p/s and *Y*) p/s. Electrode montage was high forehead to ipsilateral mastoid. The common electrode was placed on the contralateral mastoid. The response was filtered between \cdots and $\neg \cdots$ Hz, amplified Verse times, recorded over 1...75 ms time window and 7... sweeps were averaged for each run. ABR was done to exclude retrocochlear pathologies when hearing sensitivity permit ABR recording. MRI petrous bone with gadolinium was done in some patients instead of ABR when hearing loss is severe enough (> $\vee \cdot dB HL$) to preclude ABR recording.

IV-Vestibular evaluation in the form of

1- A complete VNG test battery using the ICS Chartr binocular four channel system. VNG examination included the search for spontaneous, gaze-evoked and postheadshake nystagmus. It also included the recording of smooth pursuit, saccadic and optokinetic eye movements. The search for positioning and positional nystagmus was also performed during the right and left Dix-Hallpike tests, and when patients were in the supine position (with head centered, head to the right and head to the left), right decubitus and left decubitus positions. Finally, a monothermal caloric test was conducted using cool water irrigation at *^γ*•°C^[^γ].

*****-VEMP testing was performed using IHS with Smart EP software, version \pounds .^o. The patients were tested either in the sitting position or in the supine position and head rotated away from the stimulated side during recoding. EMG activity was recorded ipsilaterally from the middle of the SCM using a surface (active) electrode, with a reference electrode on the ipsilateral sternoclavicular joint and a ground electrode on the forehead. Care was taken to place the bilateral electrodes symmetrically. During each recording session,

patients were instructed to rotate their heads towards the contralateral side away from the tested ear to keep the SCM under tension. The patients were instructed to tense the SCM during acoustic stimulation and relax it between recording sessions. The stimulus will be click $\gamma \cdot \eta$ and STB at \cdots and \cdots Hz () ms rise and fall time and ° msec plateau time). The stimulus were presented ipsilaterally through Telephonics TDH-^{£9} headphone. The EMG signal was amplified (°··· times). filtered $(1, -1, \circ, \cdot, Hz)$. bandpass The repetition rate of the stimuli was o.) stimulus/second and an average of at least γ .. sweep were taken. The intensity of each stimulus was 9°dBnHL and two waveforms were recorded for each stimulus type (click, \cdots Hz TB and \cdots Hz TB) to test wave reproducibility. The analysis window started $\tilde{\cdot}$ ms before stimulus onset and ended V. ms after stimulus onset (i.e. from -^{ψ} · msec to ^{ψ} · msec). Each ear was stimulated separately and the first ear to be tested was selected randomly.

To decrease the effect of tonic activity of the SCM on the recorded VEMP and ensure equal muscle contraction on both sides, the recording device and the Smart EP software only accepted data acquisition when the root mean square EMG activity was between $\circ \cdot$ and $1 \cdot \cdot \mu V$. Data acquisition was rejected when root mean square EMG activity was below $\circ \cdot \mu V$ or above $1 \cdot \cdot \mu V$. The level of root mean square EMG activity was monitored and appeared on the computer screen, allowing the examiner to give feedback responses to the patient to increase or decrease muscle contraction and maintain constant muscle tension.

Upon recording the waveforms, the first positive deflection was marked as P¹ and the first negative deflection will be marked as N¹. Such wave (P¹-N¹) was wave to be analyzed. The analyzed VEMP parameters for these stimuli (click, °·· Hz TB, ¹··· Hz TB) were:

i- P¹-N¹ peak to peak amplitude. ii- P¹-N¹ corrected amplitude.

Corrected amplitude of $P^{1}-N^{1}$ was used to control the differences in muscle activation. The CA was computed with the software by dividing the $P^{1}-N^{1}$ amplitude

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by the root mean square of EMG for the first r. ms before stimulus onset according

to this formula^[^].

$$CA = \frac{Raw amplitude of P1 - N1 \quad (peak to peak amplitude)}{Raw amplitude}$$

iii-P\and N\ latency

iv-\.../o.. Hz frequency peak amplitude (FPA) ratio:

which is defined as P¹-N¹ peak to peak corrected amplitude at \cdots Hz TB divided by P¹-N¹ peak to peak corrected amplitude at \cdots Hz.

$$FPA = \frac{P1 - N1 \text{ Corrected amplitude at } 1000 \text{ Hz}}{P1 - N1 \text{ Corrected amplitude at } 500 \text{ Hz}}$$

For the control subjects, AR was calculated according to such formula

$$AR = \frac{\text{Larger corrected P1} - \text{N1 amplitude} - \text{Smaller corrected P1} - \text{N1amplitude}}{\text{Sum of corrected amplitude in both ears}}$$

For the Ménière's patients, AR was calculated according to such formula

$$AR = \frac{\text{corrected amplitude of other ear} - \text{corrected amplitude of Meniere's ear}}{\text{Sum of corrected amplitude in both ears}}$$

The VEMP results for the control group served as normative data. The normative limit for VEMP parameters were calculated as mean \pm ⁷.° SD of the results of control group.

Results

1- Intact vs Absent

Using $\circ \cdot \cdot$ Hz TB, VEMP results were compared between the Meniere's group and control group. While all the control ears had intact VEMP, only $\circ (\uparrow \cdot \.)$ Meniere's ears had intact VEMP and $\uparrow \cdot$ ears $(\pounds \cdot \.)$ had absent VEMP. Such results was statistically significant as shown from Binomial test (P= $\cdot \cdot \cdot \uparrow$). On the other hand, $\uparrow \uparrow (\land \pounds \.)$ from the other ears had intact VEMP and only $\pounds (\uparrow \neg \.)$ had absent VEMP. This results was not statistically significant as shown from Binomial test (P= $\cdot \cdot \uparrow \circ \pounds$).

Y- PY-NY Corrected amplitude (CA)

Results showed that the best stimulus that produced largest amplitude was $\circ \cdot \cdot$ Hz TB followed by $\cdot \cdot \cdot$ Hz TB and lastly click in

control group. Clearly, the P'-N' CA was largest for '... Hz TB in Meniere's patients.

ANOVA test and Post hoc test were performed to compare between the Meniere's group and control group as regard P'-N' CA. The P'-N' CA was statistically smaller in both Meniere's ears and other ears as compared to the control ears (p value= \cdot . \cdot) while there was no statistical significant difference between Meniere's ear and other ears (p value = \cdot . \cdot 9).

<u> π - $\cdot \cdot \cdot /\circ \cdot \cdot$ Hz frequency peak</u> amplitude (FPA) ratio:

In the current study, FPR was considered abnormal if it was above the mean +^Y. •value of the control subjects (i.e; above •. • • •). Similar to P¹-N¹ CA, the FPA ratio in both the Meniere's ear and other ear was larger compared to the control ears while there was no statistical significant difference between Meniere's ears and other ears. Table ¹, ^Y show this results. Table 1: ANOVA for comparison between Meniere's group and Control group.

	Control	Meniere's ear	Other ear	F value	P value
$\cdots / \circ \cdots Hz$	•_٦١	• 97	1.77	15.740	*.***
FPA ratio					

Table ': Post hoc test for comparison between Meniere's ear, other ear and control group as regard $\cdots / \circ \cdots$ Hz FPA ratio.

	P value
Control vs Meniere's ear	•_• ٤٧
Control vs Other ear	•.•••
Meniere's ear vs Other ear	۰ <u>.</u> ۱۳۱

£- P1 and N1 latency

Contrally to P'-N' CA, there was no statistical significant difference between the Meniere's group (either the Meniere ear or the other ear) and control group as regard P' latency and N' latency (P value by ANOVA test= \cdot . \cdot . \cdot " and \cdot . \circ ϵ . \cdot

<u>°- AR</u>

Similar to P¹ latency and N¹ latency there was no significant difference between the Meniere's group and the control group as regard the AR (P value by independent sample T test = $\cdot \cdot \cdot \cdot \cdot \cdot$).

Discussion

TB stimulation at $\circ \cdot \cdot$ Hz tone was considered as an ideal stimulation^[1,1+], with the stimulus intensity that ranged between $1\circ-1\cdot\circ$ dB nHL or $11\circ-1\%$ dB SPL. Although the TB stimulation at $1\circ$ dB nHL was the most commonly used. For clinical diagnosis using VEMP, we recommend STB stimuli because latencies and amplitude of click were significantly different among several lab^[11,17].

So we use both click, ••• Hz and •••• Hz STB for comparison between MD group and control group, MAV group and control group in our study.

Our results show that in $\circ \cdots$ Hz TB, $1 \circ (1 \cdot 1)$ Meniere's ear had intact VEMP and $1 \cdot (\xi \cdot 1)$ absent which was statistically significant different. The other ear had $1 \cdot (4 \cdot 1)$ intact VEMP and $\xi (1 \cdot 1)$ absent

which is not statistically significant different.

In affected ear, VEMP was intact in \circ ears $(\vee \circ \ddot{?})$ by Ribiero^[\verty], $\vee \wedge$ ears $(\vee \uparrow \ddot{?})$ by Seo et al., $[^{1 \cdot i}]$, $\vee \vee \vee$ ears $(\circ i ?)$ by waele et al., $[^{1 \cdot i}]$, $\vee \vee$ and $(\circ i ?)$ by waele et al., $[^{1 \cdot i}]$, $\vee \vee$ by Murofushi $[^{1 \cdot 1}]$. Young et al., $[^{1 \cdot i}]$, de waele et al., $[^{1 \cdot i}]$ Murofushi et al., $[^{1 \cdot i}]$ reported that variation between in the incidence of intact VEMP can be explained by the different stages of MD.

Previous studies found reduced VEMP responses to clicks in Meniere subjects, with a substantial proportion of subjects showing no VEMP response $[1^{(0,1)}]$ in comparison to normal subject there was reduced amplitude in both ears of unilateral Meniere's subjects with greater changes in the affected ears as the average VEMP amplitude at the affected side is significantly lower than that at the unaffected side. It was explained by reduced VEMP amplitude at the affected side points toward a permanently affected otolith system in unilateral Meniere's patients at the side of Meniere's ear. The affection of the cochlea and part of the vestibular system are related. Kingma^{$[1^{A}]$}, Rauch et al.,^{$[1^{i}]$} which agree with our results.

Our result shows that there was no statistically significant difference between Meniere's group and control group in P¹ and N¹ latency.

There was no statistically significant difference between absolute latencies of wave P1 and N1 on affected and a symptomatic ears^{[γ}]. The same was found by young et al.,^['v], Waele et al.,^['°] observed latency of response in subjects MD similar to that of normal subjects detecting differences only in amplitude of response. These finding are similar to our results. This can be explained by that the latency depends predominantly on central signal transmission and muscle activation, is unaffected bv saccular deformation (hydrops) in Meniere's disease^{$[1, \cdot]$}.

Young et al.,^[14] reporting 1.% of cases of late endolymphatic hydrops with prolongation of absolute latency of P1, justifying these finding owing to high endolymphatic pressure that would affect the transmission of sound, provided that hearing was also affected to Murofushi et al.,^[14], prolongation of latency of P1 suggested retrolabyrinthine damage. These are against our results.

Because MD reduces VEMP responses, it might be thought that a symmetry of the VEMP response would provide a good clinical test of unilateral MD but unexpectly this difference was not statistically significant this is explained by Rauch et al.,^[1+] that there is occult disease in the unaffected ear [occult bilateral disease in Meniere's subjects] and this is similar to our results.

Our results show in both Meniere's ear and other ear FPA ratio was larger compared to control ears while no statistically significant difference between Meniere's ear and other ears. Kim-Lee^[Y+] show that $1 \cdot \cdot \cdot / \circ \cdot \cdot$ Hz FA ratio is elevated in MD and this represents a useful diagnostic criteria in the diagnosis of MD. Kim-Lee^[Y+], Rauch et al.,^[1+] suggested that the elevated FPA ratio in their VEMP responses using TB stimuli of $\circ \cdot \cdot$ and $1 \cdot \cdot \cdot$ Hz. Likely due to a shift in the morphologic features of the saccule. The change in VEMP frequency tuning produced by MD provides a clue to the origin of VEMP tuning. Welgampola and Colebatch^[Y1] suggested that VEMP tuning originated in an electrical resonance of the hair cells, whereas Todd et al.,^[YY] suggested that VEMP tuning was attributed to that VEMP tuning was attributed to the mass spring damping properties of the saccule.

We found that the FPA ratio was significantly different between patients with MD and normal subjects. So we suggest that the resultant FPA cutoff value would be clinically useful in diagnosis of MD which agree with Kim lee and Rauch et al.,

Conclusion

The altered VEMP dynamics seen in Meniere's disease offer the possibility that VEMP testing may be clinically useful in the assessment and early detector of involvement of sacculus in endolymphatic hydrops of MD, both on the affected and on the asymptomatic ear and/or monitor of evolving Meniere's disease or of the efficacy of potential Meniere's treatments.

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